

# Thermopneumatic Actuator for Tactile Displays

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**Abstract**—This paper presents a new tactile display based on thermopneumatic actuators. Since the main drawback of these devices in the market is their cost, this proposal is intended to reduce the price because of the simplicity of the actuator. This actuator has been used in micropumps and microvalves in technologies for MEMS, thus very small devices could be fabricated to improve the resolution, and circuitry and sensors could be added in the same substrate to get smart processing and actuation. A small display with activation circuitry has been built to show the viability of the proposal and preliminary experimental results of stroke and dynamic response illustrate the performance of the actuator in this first prototype.

**Index Terms**—Blind people aids, Tactile graphic displays, Thermopneumatic actuator.

## I. INTRODUCTION

Tactile displays show the information by stimulating the sense of touch. They are required as reading tools for blind people and more recently in areas like virtual reality and telesurgery. Most devices in the market are based on piezoelectric cells. However, a Braille cell (eight points) costs around 35€ and a Braille display (one line of text) costs around 10000€. The display DMD 12060 from Metec implements an array of 159 x 59 miniature solenoids with a distance of 3mm between centers and a cost around 60000€ [1]. Obviously, the main drawback of these devices is its high cost, specially for large *displacement displays* [2] which are those explored with the fingers.

A common strategy to reduce the cost in the so called *force displays* [2] is by means of a pointer device, for instance a computer mouse, and a small tactile display on it. A finger (or a few fingers) rests on the display whose content is refreshed as the mouse is moved along the so interpreted virtual tactile image. The VirtTouch mouse is based on this idea and costs around 5000€. However, the information these devices transmit to the skin is quite limited. That is because much information is collected by dynamic mechanoreceptors in the skin while the fingers explore a surface, because of the slip or tangential forces [3][4]. Thus, there is still a great interest in new actuators that allow a more efficient implementation in terms of cost and performance.

There is a wide range of possibilities, but most work is done in electrical stimulation [5][6], SMA (shape memory alloy) actuators [7][8], pneumatic [9], based on ER (electrorheological) fluids and organic gels [10][11] or based

on MEMS (Micro-Electro-Mechanical Systems) [12][13]. Electrical stimulation is an old idea but it has not got yet the desired results, although advances have recently achieved [6]. SMA wires change its length (around 5%) when heated by a current (around 2A) through them. Most problems to solve are small stroke, high power consumption, slow response, hysteresis and the need of small mechanical structures. Pneumatic devices are bulky unless they use microvalves to control the flow, for instance valves in MEMS technologies [12]. These devices are not yet mature enough although they could be a good choice in the future. The response of the ER fluids is fast (in the milliseconds range) but the resolution and stroke are poor. A pneumatic display based on these fluids has been proposed and seems to improve the performance of previous approaches [10].

In summary, much work is carried out in the development of new actuators that could lower the cost and improve the performance of tactile displays. This paper presents another alternative. It exploits the idea behind thermopneumatic microvalves and micropumps to build a simple tactile display. Although there are still many problems to be solved, the preliminary results show the viability of the proposal and encourage us to face the improvement of the actuator and control circuitry as well as the construction of a large display.

## II. THERMOPNEUMATIC ACTUATOR

Thermomechanical actuators provide good performance in terms of displacement, force and work per cycle. Thermopneumatic micropumps and microvalves are based on sealed cavities that have a flexible side [14]. The cavities are filled with a low boiling point liquid (for instance methyl chloride) and a resistive heater is built inside. When the heater increases the temperature in the cavity, the pressure grows because of the gas resulting from the liquid-gas phase transition, and the flexible side of the cavity is displaced.

This idea is proposed by the authors to build tactile displays. Fig. 1 shows the proposed actuator as built to get the preliminary results of this paper. It consists of a small cylinder made of copper with an end sealed with tin and the other with a flexible diaphragm. A signal diode has been chosen as heater due to its small size, although it can be replaced by a resistor or other semiconductor devices.

The Clapeyron's equation gives the following expression for a region close to the boiling point ( $P_B, T_B$ ),

$$P = P_o \exp\left(-\frac{l_v}{RT}\right) \quad (1)$$

where  $P_o = P_B \exp\left(\frac{l_v}{RT_B}\right)$ ,  $P$  is the vapor pressure inside the cavity,  $T$  is its temperature and  $l_v$  and  $R$  are constants.

On the other hand, the displacement  $s$  of a circular diaphragm under a pressure  $P$  is,

$$s = 0.0151(1 - \mu^2) \frac{Pa^4}{Eh^3} \quad (2)$$

where  $a$  is the radius,  $\mu$  is the Poisson coefficient,  $E$  is the Young modulus and  $h$  is the diaphragm thickness.

From (1) we conclude that the change of the pressure with the temperature is high near the boiling point, and it will be the same for the displacement in (2). Thus, we should work close to the boiling point to have the best performance. Liquids with low boiling points are required to save power in increasing the temperature up to the boiling point, although they should be higher than the ambient temperature to avoid undesired activations. In addition, the diaphragm should have small values of  $\mu$ ,  $E$  and  $h$ , i.e. it must be flexible.

As regard to the actuator in this paper, the liquid inside is acetone, with boiling point 56.2°C (phase transition in SMA devices is around 50°C) and the diaphragm has been implemented with latex. Although these choices allow us to show a display with a resolution similar to other reported proposals and preliminary experimental results point to the feasibility of the proposal, both the display and actuator are far to be optimized. Special care has to be taken to reduce leakage, which is large in this prototype because latex is permeable to acetone, thus flexible plastic diaphragms will replace the latex ones in future displays. In summary, tough task of modeling and looking for other materials is going to be done once the idea has worked well enough in this first prototype.

### III. TACTILE DISPLAY

Fig. 2 shows a prototype of display with the proposed thermopneumatic actuator. It consists of an array of 4 x 4 actuators with a distance of 2.54 mm between centers and an active area around 1 cm<sup>2</sup>. Fig. 2 (a) shows a draw with a side cut of the prototype. The thermopneumatic actuators have been mounted in a standard circuit prototyping board. Drills have been made and individual electrical control as well as a sealing mechanism have been implemented. The display is showing a 'one' in Braille at the photograph in Fig. 2(b).

Other reported displays have 4 x 4 actuators with 0.7mm diameter and separated 2mm [6], or 6 x 6 actuators with 1.5mm diameter and 16mm x 16mm display area [15], while the ideal resolution (given by human skin features) is 1 actuator per square millimeter, thus this first prototype is close to other state-of-the-art proposals in terms of spacial resolution. The

existence of micropumps based on the same thermopneumatic actuators will allow likely to build displays with ideal resolution based on this technology.

### IV. ACTUATION CIRCUITRY

The activation of the proposed actuator shares many problems with that of other actuators based on thermal principles, like SMA devices. As regard to the latter, they have hysteresis while it is not the case of the proposed actuator. However, there is also a trade-off between turn-on and turn-off times improvement. Let us use the simplified model in Fig. 3 to illustrate the design problem.

In Fig. 3,  $P$  is the electrical power dissipated by the heater (a diode in our case),  $R$  is the thermal resistance and  $C$  is introduced to model the transient behavior. For this simple model the temperature evolution during turn-on in Fig. 3(a) is

$$T = T_a + PR(1 - e^{-t/RC}) \quad (3)$$

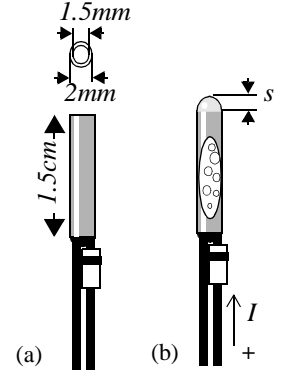


Fig. 1 Thermopneumatic actuator.

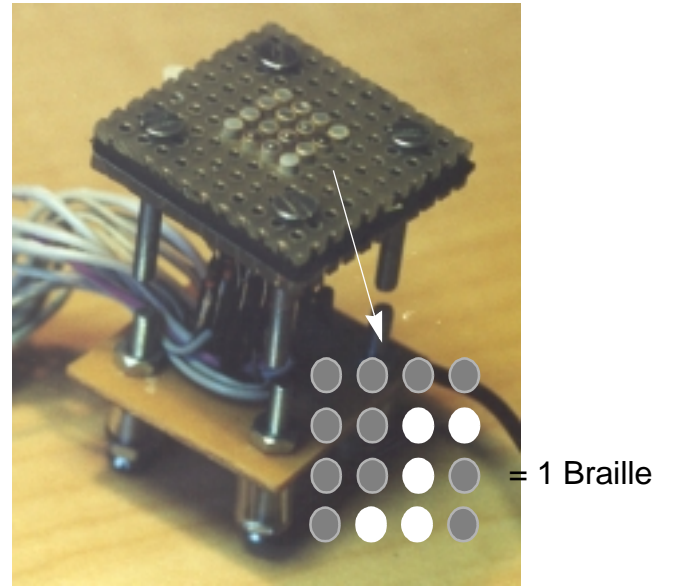
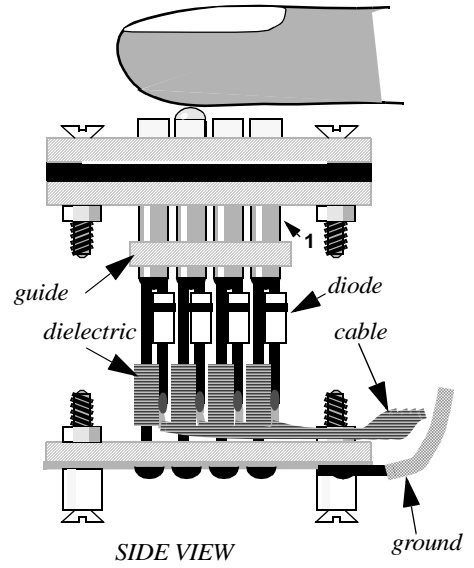


Fig. 2 Prototype of tactile display with thermopneumatic actuators.

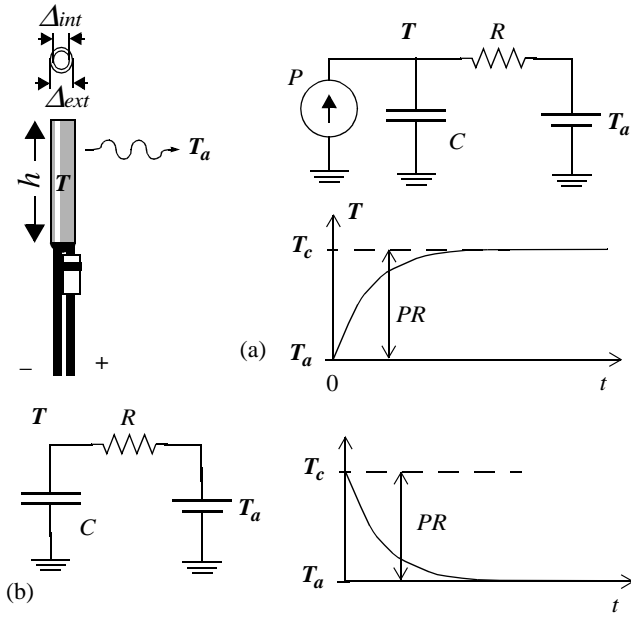


Fig. 3 Models and temperature evolution during turn-on (a) and turn-off (b).

and that for turn-off in Fig. 3(b) is

$$T = T_a + PR e^{-t/RC} \quad (4)$$

hence both follow an exponential behavior with a time constant equal to  $RC$ .  $C$  is related to the actuator volume while  $R$  is related to the actuator surface and shape. In order to reduce turn-on and turn-off times a low value of  $R$  is desired. However, this means a higher power has to be dissipated by the heater to reach the target temperature  $T_c$  (note that  $PR$  is the temperature increment in Fig. 3). Hence, low values of  $R$  and high values of  $P$  are required for a fast response.

Force displays based on SMA actuators have to be refrigerated ( $R$  is reduced) with water to work at a frequency of 30Hz. This strategy has not been implemented in the prototype of this paper. It will not be likely necessary to build a displacement display, where the frequency of operation is not essential and times of a few seconds can be tolerated. Nevertheless, a bi-level strategy has been implemented to increase the speed that consists in injecting a high power  $P_{exc}$  at the beginning of the activation to increase the temperature quickly, and a lower power  $P_{hold}$  once the actuator is active to reduce power consumption and avoid damage of the heater element.

Circuitry in Fig. 4 has been proposed to implement the bi-level strategy. The signal diode D4148 drives a current

$$I = \frac{V_{pol}}{R} = \frac{V_{DD}R_2}{R(R_1 + R_2)} \quad (5)$$

as long as the transistor  $Q_1$  is cut off. This is achieved by generating a negative pulse of duration  $\Delta$  at input. As soon as the pulse finishes and the input becomes high  $Q_1$  saturates,  $V_{pol}$  is small and  $I$  reduces to just a few mA. The rated pulse width  $\Delta$  and the current  $I$  could be obtained from the diode data sheet. However, since a copper tube is soldered to the diode the thermal resistance has been modified and data in the data sheet referred to maximum power are not longer valid and deep work

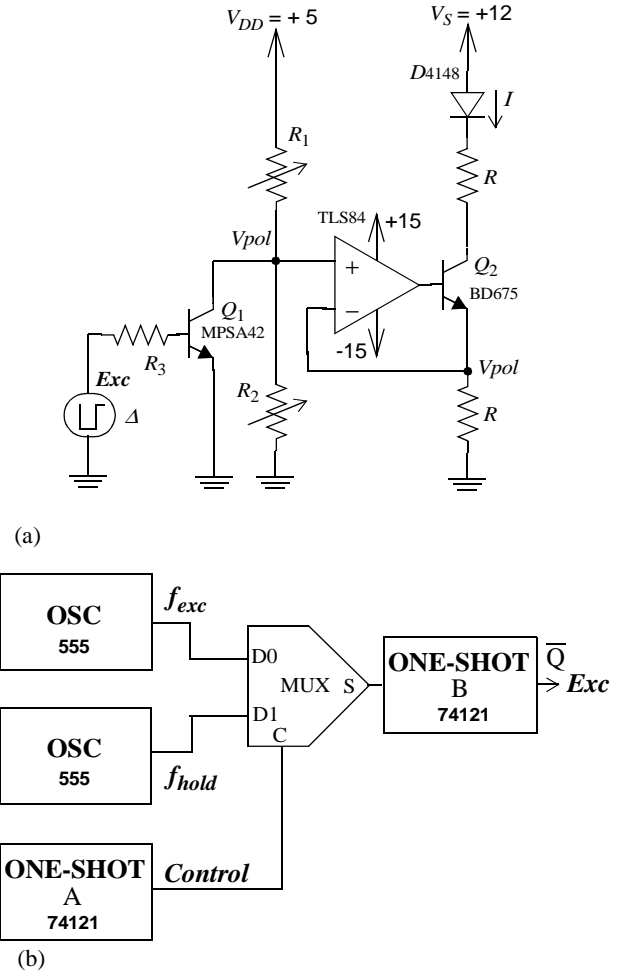


Fig. 4 Circuit to generate a current pulse (a) and circuitry to implement a bi-level strategy (b).

of thermal behavior modeling has to be done to obtain optimal performance.

A pulse train instead of a constant current is generated to feed the diode. This excitation has been found to increase quickly the temperature of power semiconductor devices. The pulse train is obtained by triggering a one-shot with an oscillator. The bi-level strategy is implemented by means of two oscillators, one to generate the high excitation frequency  $f_{exc}$  and the other to generate the holding frequency  $f_{hold}$ . A multiplexer (implemented with just 3 nand 74LS00 gates) put the proper output depending on the state of the control signal, which is generated with another one-shot. The result is a current pulse train in the diode with a frequency  $f_{exc}$  for a time controlled by the one-shot A, and a current pulse train of frequency  $f_{hold}$  after this period. The duration of every current pulse is controlled by the one-shot B (i.e. the duty cycle) and its amplitude by the resistors  $R_1$  and  $R_2$  (see Fig. 4(a) and eq. (5)).

Fig. 5 Illustrates the above description with measurements of the control signals and excitation pulses in the preliminary results of this paper. Fig. 5(a) and (b) shows the multiplexor output (top) and control signal (bottom). In addition, Fig. 5(c) and (d) shows the current pulse in the diode and the drop of voltage in it respectively.

## V. RESULTS AND DISCUSSION

Fig. 6 shows a curve that illustrates the behavior of the

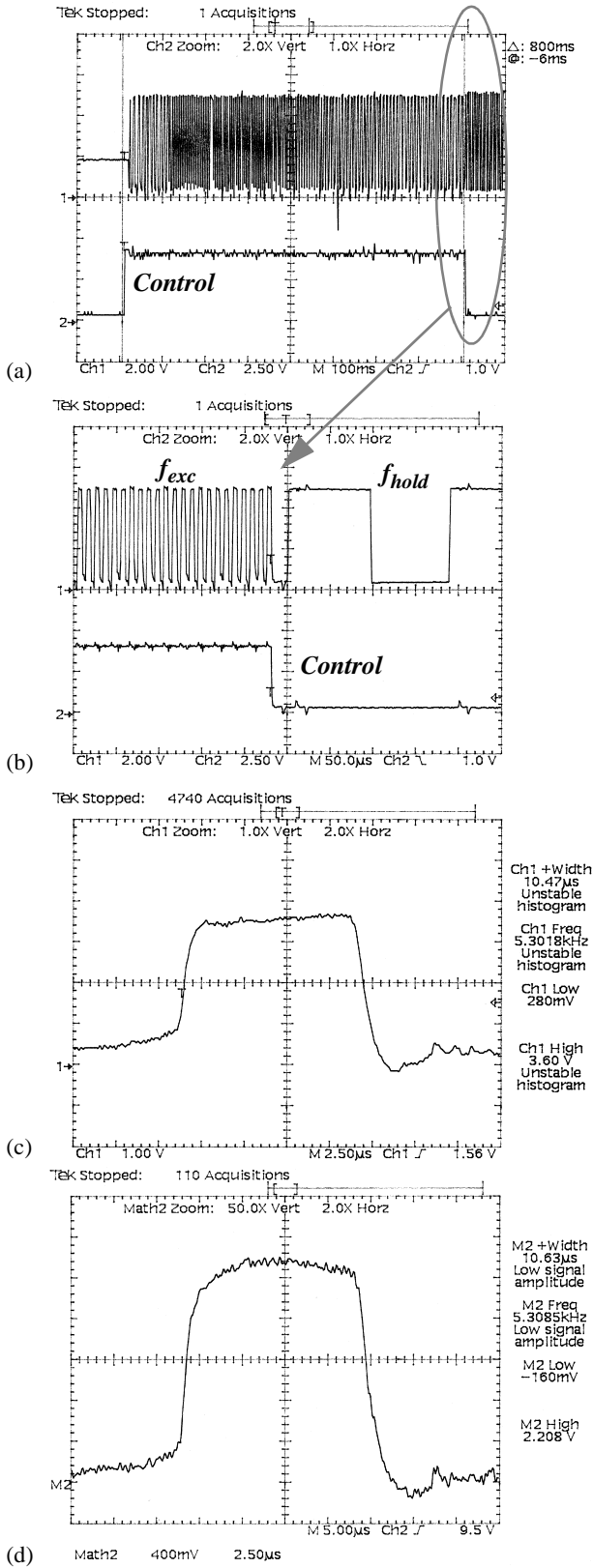


Fig. 5 Multiplexor output (top) and control signal (bottom) in the bi-level strategy (a) and (b), and current pulse (c) and voltage drop (d) in the diode.

actuator during its turn-on and turn-off. Rise and fall times are around 4 and 15 seconds respectively for  $f_{exc} = 50kHz$  and  $f_{hold} = 5kHz$ . They have been obtained by using an LDVT as displacement sensor. The sensor has been calibrated with a micrometer and it has a sensibility of 0.68 V/mm, hence the stroke of the actuator in this experiment is around 0.7mm.

Comparison with other proposals is difficult at this first stage of the research. The ideal displacement tactile display should have a resolution of one actuator per square millimeter. The DMD-12060 has a distance of 3.08 mm between centers and a standard piezoelectric cell in a refreshable tactile display has 3.21mm and 2.45mm of  $x$  and  $y$  distance between centers respectively. The 3D display in [4] has a distance of 3mm between centers. With respect to the stroke or vertical displacement, the Braille cell in a refreshable display has a stroke of 0.7mm, and the skin is able to detect shapes as thin as 0.1mm high [4]. The force of the finger against a tactel during exploration could be up to 2.35N as reported in [4] and our actuator lifts a core (that of the LVDT) of 1 gram weight, hence a equivalent force of just 0.01N. However, although further tests are obviously necessary to know the performance under harder conditions, the skin can detect forces as small as 0.001N [16]. As regard to the dynamic response, refreshing times of 15s are reported for the display in [4]. Requirements of force displays are much more restricted for dynamic response, and strategies like cooling are used to reach the desired speed. That could be the case of a force display made with the proposed actuator. With respect to a displacement display, although multiplexing can improve the performance, the power consumption could be of a few thousands of watts. Although

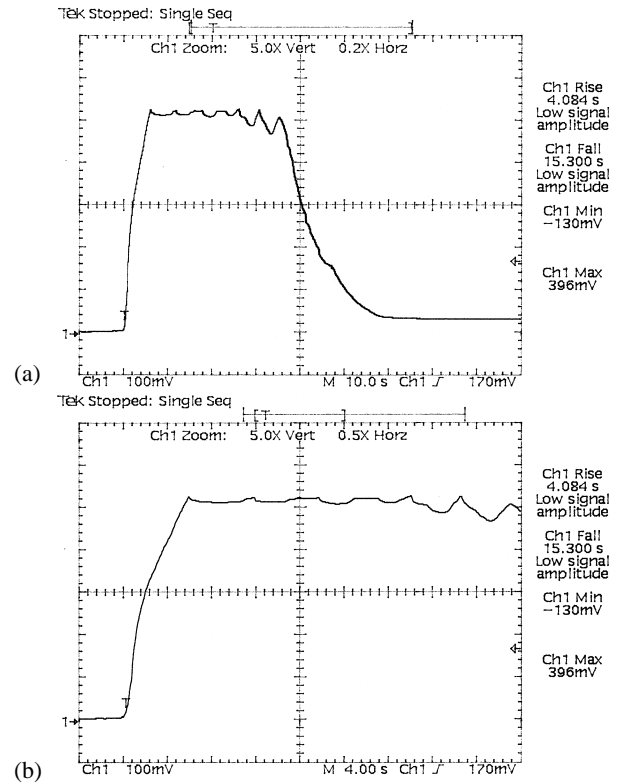


Fig. 6 Activation and deactivation response of the actuator (a) and activation detail (b).

much work has to be done to have a final prototype optimal enough to decide if it is necessary, a strategy to reduce the power consumption uses locking mechanisms to keep the tactel active without power supply.

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